

TOPOLOGICAL GRADIENT APPROACH TO EDGE DETECTION AND SPECKLE NOISE REMOVAL IN ULTRASOUND IMAGES

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Introduction

It is well-known that the ultrasound images are corrupted by the speckle noise [2]. The observed image is assumed to be positive and decomposed as follows

$$g = u + \sqrt{u}\eta,$$

where the speckle noise η is a positive function and follows the Rayleigh-distribution.

Problem formulation

Let Ω be an open subset in $\mathbb{R}^2$ is the image domain.

To remove the speckle noise from an ultrasonic image, we study the following variational denoising model

$$\min_{\{u>0, u \in H^1(\Omega)\}} \left\{ \frac{\lambda}{2} \int_{\Omega} |\nabla u|^2 dx + \int_{\Omega} \frac{(g-u)^2}{u} dx \right\}, \quad (1)$$

where $\lambda > 0$ is a weighting factor between the regularization term and the data fidelity term. The associated Euler-Lagrange equation is given by

$$\begin{cases} -\operatorname{div}(\lambda \nabla u_0) + \frac{u_0^2 - g^2}{u_0^2} = 0, & \text{in } \Omega, \\ \partial_n u_0 = 0, & \text{on } \partial\Omega. \end{cases} \quad (2)$$

where ∂_n denotes the normal derivative and n is the outward unit normal to $\partial\Omega$.

This equation admits a unique solution u_0 in $H(\Omega) := \{u > 0; u \in H^1(\Omega)\}$.

Edge detection: Among several techniques proposed to **restore** the speckle noise arising in medical ultrasonic image, we resort, in this poster, to **the topological gradient method** [1].

The topological sensitivity analysis

- For a small parameter $\rho > 0$, let $\Omega_\rho = \Omega \setminus E_\rho(x_0)$ be the perturbed domain obtained by removing an ellipse of size ρ around the point x_0 .
- The topological asymptotic expansion of $j(\Omega)$ when ρ goes to zero is the following

$$j(\Omega_\rho) - j(\Omega) = \rho^2 \mathcal{G}(x_0) + o(\rho^2),$$

where $\mathcal{G}(x_0)$ is called the topological gradient at x_0 .

- To preserve the edges of an image and smooth it elsewhere, we compute the asymptotic expansion of the following cost function

$$j(\Omega_\rho) = J(u_\rho) = \frac{1}{2} \int_{\Omega_\rho} |\nabla u_\rho|^2 dx, \quad (3)$$

where u_ρ is the solution of the following perturbed equation

$$\begin{cases} -\operatorname{div}(\lambda \nabla u_\rho) + \frac{u_\rho^2 - g^2}{u_\rho^2} = 0, & \text{in } \Omega_\rho, \\ \partial_n u_\rho = 0, & \text{on } \partial\Omega_\rho. \end{cases} \quad (4)$$

- The Topological gradient $\mathcal{G}(x_0)$

$$\mathcal{G}(x_0) = -\pi \left(ab \left(1 - \frac{g^2(x_0)}{u_0^2(x_0)} \right) (v_0(x_0) - u_0(x_0)) + \lambda(a+b) \nabla u_0(x_0) \cdot \mathcal{P} \nabla v_0(x_0) \right),$$

where

$$\mathcal{P} = \begin{pmatrix} b \cos^2 \varphi + a \sin^2 \varphi & (a-b) \cos \varphi \sin \varphi \\ (a-b) \cos \varphi \sin \varphi & b \sin^2 \varphi + a \cos^2 \varphi \end{pmatrix},$$

for all $\varphi \in [0, 2\pi]$ and $a, b > 0$ are the lengths of the semi-axes of E .

The adjoint problem

The function v_0 defined in the topological gradient formula is the solution of the following adjoint problem

$$\begin{cases} -\operatorname{div}(\lambda \nabla v_0) + \frac{2g^2}{u_0^3} v_0 = \frac{u_0^2 + g^2}{u_0^2}, & \text{on } \Omega, \\ \partial_n v_0 = 0, & \text{in } \partial\Omega. \end{cases} \quad (5)$$

If we take $a = b = 1$, we find the topological gradient for a perforated domain by a ball.

When we take $a = 1$ and tend b to zero, we find the topological gradient for a cracked domain.

Restoration algorithm

The steps of the algorithm are the following:

- Initialize: $\lambda = \lambda_0$.
- Compute u_0 : the solution of equation (2).
- Compute v : the solution of equation (5).
- Compute the topological gradient $\mathcal{G}(x_0)$ for each point $x_0 \in \Omega$.
- Take $\lambda = \begin{cases} \lambda_1 & \text{if } x_0 \in \{x \in \Omega \text{ such that } \mathcal{G}(x_0) < \alpha < 0\}, \\ \lambda_0 & \text{otherwise } (\lambda_1 \ll \lambda_0). \end{cases}$
- Compute u_0 with the new value of λ .

where α is a given negative threshold.

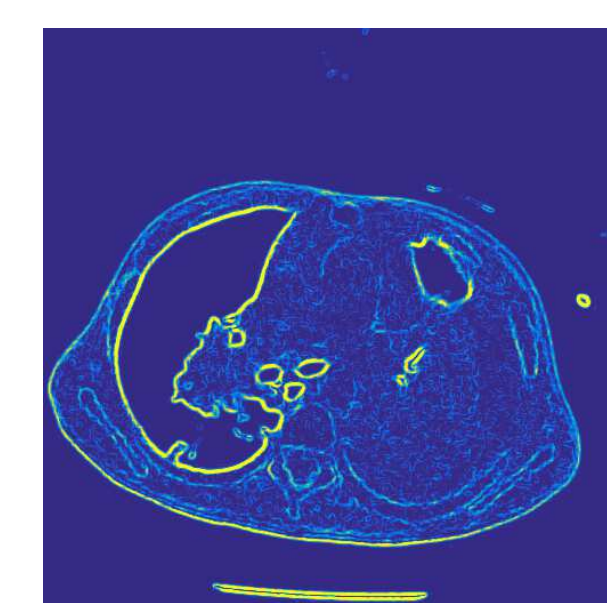
Numerical examples

From left to right: Noisy image, contour and restored image, respectively.

•Chest image



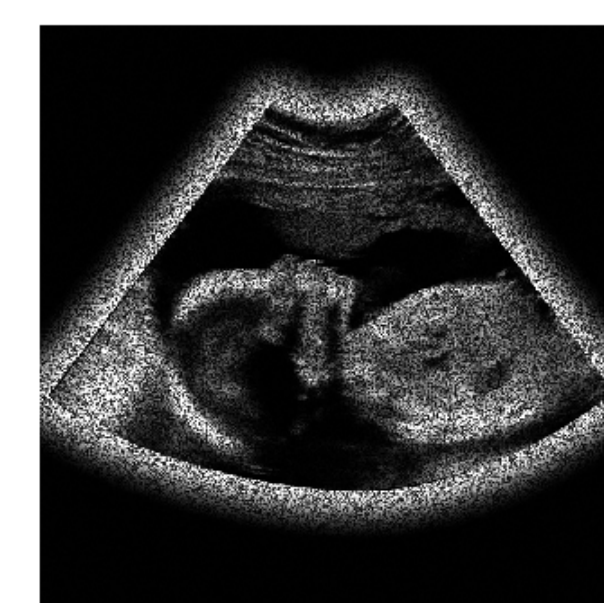
snr=11.88dB, ssim=0.72



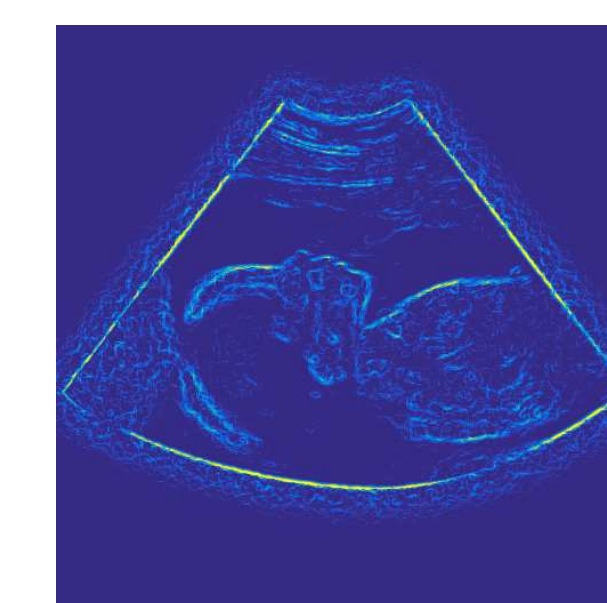
snr=18.74dB, ssim=0.88

The edges obtained by the topological gradient with threshold $\alpha = -200$ and the recovered image with $\lambda = 1.7$.

•Sonography image



snr=6.54, ssim=0.63



snr=16.01dB, ssim=0.87

Conclusion and references

Conclusion

- We have studied a new method based on the topological sensitivity approach to remove speckle noise in ultrasound images.
- The edges are well preserved and the image is smoothed elsewhere during the restoration process.
- We can consider a similar approach for a higher-order PDE in Ultrasound Computed Tomography.

References

- [1] A. Drogoul and G. Aubert, The topological gradient method for semi-linear problems and application to edge detection and noise removal, *Inverse Problem and Imaging*, **10** (2016), 51–86.
- [2] Z. Jin and X. Yang, A variational model to remove the multiplicative noise in ultrasound images, *J. Math. Imaging Vis.*, **39** (2011), 62–74.